

Changes in shoulder muscle size and activity following treatment for breast cancer

Delva R. Shamley · Ragavan Srinanaganathan · Rosamund Weatherall · Reza Oskrochi · Marion Watson · Simon Ostlere · Elaine Sugden

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Abstract

Background Morbidity of the shoulder after breast cancer is a well-known phenomenon. MRI studies have shown muscle morbidity in cervical cancer and prostate cancer. In breast cancer clinical observations and patient reports include muscle morbidity in a number of muscles acting at the shoulder. Several of these muscles lie in the field of surgery and radiotherapy. Timed interaction between muscles that stabilise the shoulder and those acting as prime movers is essential to achieve a smooth scapulohumeral rhythm during functional elevation of the arm.

Method: Cross-sectional study Seventy-four women treated for unilateral carcinoma of the breast were included in the study. All patients filled out the Shoulder Pain and Disability Index (SPADI). EMG activity of four muscles was recorded during scaption on the affected and unaffected side. Muscle cross sectional area and signal intensity was determined from

MRI scans. The association between EMG and covariates was determined using multiple linear regression techniques.

Results Three of the 4 muscles on the affected side demonstrated significantly less EMG activity, particularly when lowering the arm. Upper trapezius demonstrated the greatest loss in activity. Decreased activity in both upper trapezius and rhomboid were significantly associated with an increase in SPADI score and increased time since surgery. Pectoralis major and minor were significantly smaller on the affected side.

Conclusion Muscles affected in the long term are the muscles associated with pain and disability yet are not in the direct field of surgery or radiotherapy. Primary muscle shortening and secondary loss of muscle activity may be producing a movement disorder similar to the ‘Dropped Shoulder Syndrome’. Exercise programmes should aim not only for range of movement but also for posture correction and education of potential long-term effects.

D. R. Shamley (✉) · R. Srinanaganathan
Department of Physiotherapy, School of Health and Social Care, Oxford Brookes University, Jack Straws Ln, Marston, Oxfordshire OX3 0FL, UK
e-mail: drshamley@brookes.ac.uk

R. Weatherall
Centre for Statistics in Medicine, Oxford, UK

R. Oskrochi
Department of Mathematical Sciences, Oxford Brookes University, Oxford, UK

M. Watson · S. Ostlere
MRI Unit, Nuffield Orthopaedic Hospital, Oxford, UK

E. Sugden
Department of Oncology, Churchill Hospital, Oxford, UK

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Introduction

Breast screening programmes have allowed more conservative approaches to surgery and radiotherapy for women diagnosed with breast cancer [1]. Despite the use of less extensive surgery and where possible the avoidance of radiotherapy to the axilla, there is still morbidity affecting the shoulder [2–4]. Radiotherapy is standard practice for patients receiving conservative surgery and those at risk of recurrence, and is generally

given in 3–5 weekly sessions for up to 6 weeks. The high energy X-rays interact with molecules of the tissues causing ionisation and the release of electrons resulting in secondary damage to adjacent tissues. Radiation injury to normal tissues is believed to be non-specific and generally to produce no pathognomic changes [5]. However, the combined changes in the parenchyma and vascular tissues [6, 7] are thought to characterise the radiation damage to healthy tissues. Changes in the vascular network are thought to cause muscle ischaemia whilst a limited ability to expand, due to connective tissue constraints, is believed to have an effect on the efficacy of muscle contraction [8–10]. Most studies have found axillary radiation to be a prognostic factor for the development of shoulder morbidity [3, 4, 11]. Soft tissue changes have been seen from the onset of radiotherapy (dose dependent) to as late as 3 years after the start of radiotherapy [6, 7]. MRI studies have shown radiation induced muscle morbidity in cervical cancer [9] and prostate cancer [7]. In breast cancer only clinical observations have been reported for muscle morbidity of pectoralis major [6, 10], serratus anterior and latissimus dorsi [12]. A few studies have highlighted, but not quantified, winging of the scapula in patients demonstrating limited shoulder movements [10, 12]. Conversely, surgery alone does not eradicate arm morbidity, with 19% of patients showing reduced mobility and 39% overall arm morbidity after axillary dissection without radiotherapy [13].

Evaluation of the altered shoulder movement in breast cancer patients has been in the form of clinical observations and goniometric measures of glenohumeral range of movement [3, 13–15]. However, elevation of the arm is a function of both glenohumeral movement and scapulo-thoracic movement [16] which ensures that functional activities can occur without the head of the humerus impacting on the coracoacromial arch and placing the soft tissue structures traversing the shoulder joint, in danger of impingement. The absence of osseous stability at the glenohumeral joint means that the shoulder complex relies on the interaction of both static and dynamic structures to provide joint stability. Muscles of the shoulder form the dynamic structures and can be divided functionally into stabilisers and prime movers. Timed interaction between these two groups of muscles is essential to achieve a smooth scapulohumeral rhythm [16] and movement disorders at the shoulder have been described by several authors [11, 17–20].

The primary aim of this study was to describe shoulder muscle activity (EMG) levels and size (MRI) following treatment for breast cancer and explore the relationship of these findings to the patients report of

shoulder pain and function. Secondary aims were to identify the effects of age, handedness, surgical type, adjuvant therapy and duration since surgery on the altered size and activity.

Method

This was a cross sectional study of patients treated for breast cancer. Ethical clearance was granted by the Oxfordshire Local Research Ethics Committee (A02,064). The patients included in this study are a subset of a sample from a larger study evaluating shoulder muscle activity, joint kinematics and patients pain and dysfunction.

Participants

A sample size of 25 patients was calculated to determine a difference of 10% of voluntary muscle contraction [21], and a Sd of 0.018 (80% power; $\alpha = 0.05$, two-tailed test).

Seventy-four women meeting the inclusion and exclusion criteria (Table 1) consented to take part in the study. The time since surgery ranged from 6 months to 6 years. 57 patients consented to a MRI scan.

Glenohumeral elevation—The Polhemus Fastrak™

Glenohumeral elevation in degrees was measured using an electromagnetic position and orientation

Table 1 Inclusion and exclusion criteria

Inclusion criteria	Exclusion criteria
Unilateral carcinoma of the breast Treatment protocols*	Reconstructive surgery Current or previous history of shoulder complex trauma, surgery, pathology or dysfunction
(1) Mastectomy (2) Mastectomy + radiotherapy (3) Mastectomy + radiotherapy + axillary radiotherapy (4) Wide local excision + radiotherapy (5) Wide local excision + axillary radiotherapy + radiotherapy (6) Wide local excision + axillary clearance + radiotherapy	Lumpectomy Lymphoedema Current or previous history of cervical neuropathy

* Mastectomy included modified radical mastectomy, radiotherapy = radiotherapy to the trunk

movement tracking system. This comprises a three axis magnetic dipole source (or transmitter) and a three axis magnetic sensor (or receiver), together with related electronic equipment. The sensors are small and lightweight. Within a 76 cm source- to- sensor separation, the RMS system accuracy is 0.15 degree for orientation and 0.3–0.8 mm for position [21, 22]. The transmitter generates a low frequency magnetic field composed of three sequential excitation states, each of which produces an independent excitation vector.

All patients filled in a Shoulder Pain and Disability Index (SPADI) questionnaire immediately prior to EMG measurements being taken. The SPADI is a valid measure of pain and disability for shoulder dysfunction with high levels of sensitivity and reliability [23, 24]. The scale is a visual analog scale with 13 items (5 for pain and 8 for disability). Scores for pain range from a minimum of 0 mm to a maximum of 500 mm and for disability 0– 800 mm. 0 representing no symptoms of pain or disability.

Measurement of muscle activity

EMG protocol

EMG sensor leads were attached to the skin with the patient in standing. The patient was asked to elevate their arm in the plane of the scapula, taken as 40° anterior to the coronal plane (scaption). Both arms were taken through 3 repeat movements of scaption, each one matched to a metronome at one complete cycle every 8 s and guided to remain in this plane by a flat surface oriented 40° anterior to the coronal plane.

EMG instrumentation

This is a measure of the timing and level of muscle activity during arm movements. EMG data was collected with round pre-gelled silver-silver chloride surface electrodes (Maersk Medical). Signals were amplified with TEL 100 amplifier (Biopac Systems Inc) with a gain of 2000, a maximum input impedance of 10 K Ω was allowed, and a common mode rejection ratio of 110 dB at 60 Hz. Raw EMG signals were collected at a sample rate of 2000 Hz, and monitored throughout data collection to verify signal quality. Data was processed by MotionMonitor™ software.

Pre gelled electrodes were applied to prepared skin sites. The reference electrode was placed on electrically neutral tissue. Surface electrodes were placed parallel with the muscle fibres of pectoralis major (Pmaj), serratus anterior (SA), upper trapezius (UT) and rhomboid (Rhom) muscles as previously described

[25]. Pectoralis minor (Pmin) was not included due to tissue depth and the use of surface electrodes. EMG signal quality was verified by having the participant perform a resisted contraction in the manual muscle test position specific to each muscle being investigated.

To minimise collection of ambient noise from the VDU screen and fluorescent lights, subjects were positioned 2 m from the computer and all lights turned off.

MRI measurements

MRI protocol

The patient was scanned in a relaxed supine position with both arms at the sides and palms facing down.

STIR images at thoracic levels T2, T4 and T6 were selected as points of measure as all muscles were present at these 3 levels (pectoralis minor was missing from T2 in many patients but not all). Bilateral cross sectional area (cm³) was measured for pectoralis major, pectoralis minor, rhomboid major and serratus anterior. Upper trapezius was excluded in the clinical MRI protocol and could not be measured.

Analysis of muscle fat and connective tissue content was performed on coronal STIR images by measurement of signal amplitude in the muscle of interest and compared to the signal amplitude of the same muscle on the unaffected side.

MRI instrumentation

Scans were acquired on a Siemens 1.5 tesla Symphony using a combination of spin array and bony array receiver coils. A large field view localiser was obtained followed by (1) Coronal T1 weighted (2) Coronal STIR (3) Axial; T1 weighted and (4) Axial STIR sequences. Sections were sampled with an interslice gap of 6 mm, and 256² matrix; repetition time/echo (TR/TE) for STIR sequences was 6820/86; inversion time was 150.

Reliability

EMG data collection was carried out by the same two observers (one applied sensors to patient and gave instructions, one operated the computer) blind to the SPADI data. Intrarater reliability was assessed by carrying out repeat measures on a different day for all movements for a random sample of 5 participants. MRI measurements were taken by a single observer blind to the clinical history. Intrarater reliability was assessed by repeated measures of 10 of the 56 scans.

Data reduction and analysis

Descriptive analyses were conducted to assess demographic and clinical characteristics of the sample.

SPADI

Descriptive analysis was performed to determine contributions by individual items score to final score. A one-way ANOVA was conducted to compare the individual items on the pain and disability indices for each of the time scales since surgery (0–2 years, 2–4 years, 4–6 years).

EMG

A normalisation reference was collected for 1 min at rest for each muscle. Following this, average root mean square (RMS) movement values minus the RMS resting value were determined. Maximum Voluntary Contraction was not carried out due to the levels of pain experienced by participants. EMG data was taken at 10° increments of glenohumeral elevation (Fastrak data) and averaged for the three movements.

Owing to the observed variation between participants EMG readings during data collection, scatter plots of EMG data for each muscle for individual participants were first plotted against humeral elevation. The number of data points for the affected side lying above (more active) or below (less active) the unaffected side was expressed as frequencies and an average recorded.

MRI

Three repeat measures for each muscle and each participant were taken and the mean of the three measures used for analysis.

Paired *t*-test was used to determine the difference between muscle size and signal intensity of affected versus unaffected sides.

Blind bilateral clinical evaluation of scans were documented by SO and analysed independently by DS. Diagnoses relevant to the involved arm only were included in analysis.

Multivariate analyses

Initial exploratory analysis was carried out, plotting EMG values for each muscle and each patient separately. The EMG values for each muscle for affected

minus unaffected sides were then analysed using multiple linear regression models. As well as the degree of elevation and direction of movement (“trend” in tables), the following demographic and clinical variables were included in the analysis: age, time in days from surgery, medical treatment protocol, SPADI and handedness. Backwards-stepwise selection was applied to establish the subset of covariates with highest associations with EMG, using a *P*-value set at 0.005 for inclusion.

Bland–Altman methods were used to determine intra-rater reliability for MRI and EMG measures.

Results

Demographic and medical details are shown in Table 2. The numbers of participants with dominant and non-dominant sides affected were closely represented.

Inter-rater reliability was good for both MRI ($r = 0.89$) and EMG ($r = 0.98$) measurements.

SPADI scores as a function of duration since surgery are shown in Table 3.

No significant difference between years was found but year 4–6 shows a higher score for pain.

In rating pain, 3 items emerged as the main contributors to the total score for pain. These were ‘reaching up to a shelf’ (0–2 years, 23.4%; 2–4 years 27.2%; 4–6 years, 25.57%); ‘lying on involved side’ (0–2 years, 22.66%; 2–4 years, 23.9%) and ‘pushing an object with involved arm’ (4–6 years, 20.22% of total).

Table 2 Demographic and clinical data for study sample ($n = 74$)

	Descriptive values
Number of patients	74
Duration since surgery – mean years (sd)	3.29 (1.18)
Age – mean years (sd)	59.43 (8.86)
<i>Affected side</i>	
Left	45.9%
Right	54.1%
Mastectomy	6.8%
Mastectomy + radiotherapy	9.5%
Mastectomy + radiotherapy + axillary radiotherapy	13.5%
Wide local excision + radiotherapy	36.1%
Wide local excision + axillary radiotherapy + radiotherapy	8.1%
Wide local excision + axillary clearance + radiotherapy	27.0%
Total SPADI score – mean (sd)	187.41 (191.01)

Table 3 Pain and disability scores as a function of time intervals

Groups	<i>N</i>	Minimum (mm)	Maximum (mm)	Mean (mm)	Std. Deviation (mm)	Between group <i>P</i> -value	
Pain 0–2 years	11	0.00	230.00	96.63	76.39	0.068	
Pain 2–4 years	36	0.00	362.00	70.58	87.73		
Pain 4–6 years	27	0.00	295.00	111.92	122.00		
Dysfunction 0–2 years	11	0.00	250.00	79.45	64.53		0.159
Dysfunction 2–4 years	36	0.00	325.00	74.52	89.89		
Dysfunction 4–6 years	27	0.00	367.00	122.00	119.31		

Similarly, functional ratings revealed 2 items as contributing towards the majority of the final score. These were ‘placing object on high shelf (0–2 years, 27.6%; 2–4 years, 27.95%; 4–6 years, 27%) and ‘carrying an object of 10pounds or more’ (0–2 years, 20.7%; 2–4 years, 21.09%; 4–6 years, 22.9%). In years 4–6 an additional item emerges, ‘washing back’, which contributes 14.75% towards total score.

MRI data

Only pectoralis major and minor demonstrated a decrease in size on the affected side (Table 4). No significant difference was found in the signal intensity of any of the muscles.

Clinical diagnoses that were limited to the affected side only, were made in only 15.7% ($n = 9$) of patients (Table 5).

EMG data

Analysis of scatter plots of muscle EMG against humeral elevation for each participant showed a difference between affected and unaffected side for the majority of cases (Table 6). However, a great variation within participants and between participants, with a spread of data, was also observed. Because of the potential for outliers to cancel any mean difference, a linear regression model was fitted to the data (Tables 7–10).

Three of the 4 muscles were less active on the affected side, confirming the descriptive statistics shown in Table 6. A much larger difference was found in UT and although a difference was found for PMaj in Table 6 this

Table 4 Paired *t*-test for total mean muscle area (cm³) from MRI scans

	<i>N</i>	<i>t</i>	Sig. (2-tailed)
Pec major	57	2.177	0.034
Pec minor	57	2.289	0.026
Rhomboid	57	0.276	0.783
Serratus Anterior	57	0.690	0.493

was not shown to be significant. The covariates degree, trend and duration since surgery were significantly associated with a loss of EMG activity for all muscles. Loss of muscle activity is enhanced on the downward movement (‘Trend’ in all tables and concurs with Table 6), at the highest point of elevation (degree) and the longer the time since surgery. A high SPADI score was only significantly associated with loss of muscle activity in UT and Rhom (Tables 9, 10). Lower PMaj, UT and Rhom muscle activity were significantly associated with treatment protocol 2 (mastectomy and radiotherapy). Loss of activity in UT was significantly associated with all treatment protocols except mastectomy. Treatment protocol 3 (Mastectomy + radiotherapy + axillary radiotherapy) and 6 (WLE + axillary clearance + RT) were significantly associated with a loss in muscle activity in UT and Rhom. SA activity was lower with treatment protocol 6 but higher with protocol 3.

Discussion

This study has shown generalised loss of activity in four key muscles acting on the shoulder complex during elevation of the arm and long term pain and disability.

This concurs with previous studies showing patients who develop pain after treatment for breast cancer experience diminished ability to carry out ADL tasks, reduced health-related QOL, and psychosocial distress [26–28]. Pain scores of >30 mm have a moderate effect on ADL and scores between 30–50 mm have a severe effect on ADL [26]. This study clearly shows pain levels at all time intervals to be above 50 mm, with years 4–6 since surgery recording the highest pain scores. The main activities affected are reaching up or carrying heavy loads, which agree with findings of Karki et al. [29].

The drop in muscle activity found here supports patients reports of weakness as shown by Isaksson and Feuk [30] and Karki et al. [29], where 13% and 17.7% of patients reported weakness respectively. The lower activity in UT concurs with the observation during analysis of the MRI scans of a high number of dropped

Table 5 Patients presenting with a clinical diagnoses from MRI scans for affected side only

Case	Duration since surgery	Age	Affected side Right = R	Dominant side Right = R	Treatment	SPADI pain 500 mm	SPADI Disability/ 800 mm	SPADI Total/ 1300 mm	Clinical diagnosis
23	1525	56	L	L	mastectomy + rt + axillaryrt	28	12	40	Fluid in Subacromial bursa
232	886	48	L	R	wle + axillary clearance + rt	218	270	488	Fluid in subscapularis
268	1770	57	R	R	wle + rt	189	274	463	OA AC, glenohumeral and SC joints
288	1014	66	R	R	wle + axillary clearance + rt	35	24	59	High signal in fat plane
506	602	75	R	R	mastectomy + rt + axillaryrt	48	67	115	Signal changes biceps tendon
635	1665	55	L	R	mastectomy + rt	9	90	99	OA glenohumeral joint/subacromial cyst.
722	1967	65	R	R	wle + axillary clearance + rt	294	367	661	Moderate OA SC joint
729	986	72	R	R	wle + axillary clearance + rt	39	80	129	Fluid in subacromial bursa/full thickness rotator cuff tear.
778	950	61	R	R	wle + axillary clearance + rt	96	68	164	OA AC joint

OA = osteoarthritis AC = acromioclavicular SC = sternoclavicular

Table 6 Summary of descriptive analyses of EMG scatter plots

	Pmaj		UT		SA		Rhom	
	Arm up	Arm down						
No clear difference %	28.4	21.6	24.3	20.3	17.6	17.6	16.2	10.8
Affected side less active %	39.2	44.6	52.7	52.7	47.3	48.6	48.6	54.1
Affected side more active %	28.4	33.8	23.0	27.0	35.1	33.8	35.1	35.1

Frequency (%) of data points for affected arm above or below data points for unaffected arm

Table 7 Multiple regression for associations between Pectoralis Major EMG and covariates

PMaj emg	Coef	SE	T	P > (t)	95% conf. Interval	
Mast + RT	-8.377	1.10	-7.58	0.000	-10.545	-6.210
Degree	.108	.009	11.49	0.000	.090	.127
Trend(up/down)	-5.563	.643	-8.59	0.000	-6.811	-4.281
Days from surgery	-.003	.001	-4.02	0.000	-.005	-.002
Left handed	-3.754	1.116	-3.36	0.001	-5.943	-1.565

Mast = mastectomy RT = chest radiotherapy

shoulders (in the presence of a straight thoracic spine) on the affected side. Significant loss of all muscle activity on the downward movement of the arm indicates loss of eccentric muscle control of the shoulder girdle against gravity. Several shoulder movement disorder syndromes have been described by Sahrman [20] and include the 'Dropped Shoulder Syndrome'. This syndrome includes decreased UT activity, dropped shoulder, neck-shoulder pain, small pectoralis major and minor, numbness, symptoms aggravated by heavy breasts, heavy arms and carrying heavy objects. Some of the symptoms are believed to be due to

pressure in the thoracic outlet space (eg. Numbness, parasthesia) [20].

This study has shown decreased activity of UT, small PMaj and minor, reports of increased pain with carrying objects and lifting the arm. Similarly, the Karki [29] study at 1 year follow up demonstrated that 40.6% of patients reported neck-shoulder pain, 49% reported increased symptoms with carrying objects, and patients with a higher BMI and heavier arms had symptom exacerbation. It would appear that some patients treated for breast cancer are showing many signs and symptoms of a 'Dropped Shoulder Syndrome'.

Table 8 Multiple regression for associations between Serratus Anterior EMG and covariates

SA emg	Coef	SE	<i>T</i>	<i>P</i> > (<i>t</i>)	95% conf. Interval	
Affected or not	-3.274	.977	-3.35	0.001	-5.191	-1.358
Degree	.330	.014	22.99	0.000	.302	.358
Trend(up/down)	-5.817	.977	-5.95	0.000	-7.733	-3.901
Days from surgery	-0.005	.001	-4.57	0.000	-.008	-.003
Age	-0.191	.057	-3.33	0.001	-.303	-.078
Wle + axcle	-4.568	1.147	-3.98	0.000	-6.817	-2.318
Mast + RT + axRT	12.238	1.528	8.01	0.000	9.241	15.235

Mast = mastectomy wle = wide local excision axcle = axillary clearance axRT = axillary radiotherapy RT = chest radiotherapy

Table 9 Multiple regression for associations between Upper Trapezius EMG and covariates

UT emg	Coef	SE	<i>T</i>	<i>P</i> > (<i>t</i>)	95% conf. Interval	
Affected or not	-12.407	1.492	-8.32	0.000	-15.332	-9.483
Degree	.291	.022	13.22	0.000	.248	.334
Trend(up/down)	-26.721	1.491	-17.92	0.000	-29.646	-23.797
Days from surgery	.011	.002	6.03	0.000	.007	.014
SPADI	-.024	.004	-5.56	0.000	-.032	-.015
Mast + RT	-11.130	3.925	-2.84	0.005	-18.825	-3.434
Mast + RT + axRT	-25.170	3.746	-6.72	0.000	-32.515	-17.826
Wle + RT	-25.334	3.387	-7.48	0.000	-31.976	-18.693
Wle + RT + axRT	-26.913	4.074	-6.61	0.000	-34.900	-18.927
Wle + axcle	-24.058	3.448	-6.98	0.000	-30.818	-17.298

Mast = mastectomy wle = wide local excision axcle = axillary clearance axRT = axillary radiotherapy RT = chest radiotherapy

Table 10 Multiple regression for associations between Rhomboid EMG and covariates

	Coef	SE	<i>T</i>	<i>P</i> > (<i>t</i>)	95% conf. interval	
Affected or not	-4.739	1.111	-4.27	0.000	-6.917	-2.561
Degree	.344	.016	21.03	0.000	.312	.377
Trend (up/down)	-12.154	1.111	-10.94	0.000	-14.332	-9.975
Days from surgery	-.007	.001	-5.51	0.000	-0.010	-.005
SPADI	-.020	.003	-6.50	0.000	-.026	-.014
Mast + RT	-6.903	2.095	-3.29	0.001	-11.012	-2.794
Mast + RT + axRT	-8.760	1.796	-4.88	0.000	-12.282	-5.239
Left side affected	4.714	1.170	4.03	0.000	2.420	7.008
Wle + RT + axRT	-6.986	2.227	-3.14	0.002	-11.353	-2.619
Wle + axcle + RT	-5.637	1.370	-4.11	0.000	-8.323	-2.951

Mast = mastectomy wle = wide local excision axcle = axillary clearance axRT = axillary radiotherapy RT = chest radiotherapy

Pectoralis muscles and serratus anterior are in the field of surgery and radiotherapy and it is therefore not surprising they are affected. A short pectoralis minor muscle acts to tilt the scapula anteriorly while a weak serratus anterior will cause winging of the medial border of the scapula, confirming clinical observations. Reduction in size of PMaj may affect the patients ability to reach up, particularly as extensibility of this muscle is required to disengage the humeral head from the glenoid cavity at the end of humeral elevation [16]. However, the largest change was in UT and Rhom neither of which are in the line of surgery or radiotherapy. These 'secondary' effects noted here for up to

6 years after treatment are corroborated by patients reporting weakness for up to 5 years after treatment [30]. Furthermore, in our study patient levels of pain and functional ability were only associated with reduced UT and Rhom activity. Both UT and Rhom have lower activity associated with most of the treatment protocols. It would appear therefore that secondary muscle changes are occurring and these persist for longer and are associated with the patients ability to perform pain free functional tasks.

However, 25% of patients reported no pain and 20.27% reported no disability. Only 5% of those reporting pain did not report disability, linking pain to

the inability to perform functional movements. The question remains as to why some women experience pain and disability and others do not.

Risk factors for chronic pain include more invasive surgery, radiotherapy and acute postoperative pain [29, 30]. Patients experiencing acute postoperative pain may be inclined to adopt protective postures (dropped and rounded shoulder and arm) and reduced use of the arm, resulting in long term changes to muscle length and activity. Acute postoperative pain is most likely to occur in patients experiencing high levels of preoperative anxiety [31] and it is feasible that these women are the ones most likely to move less and protect the arm and treatment site for fear of damaging themselves further. This may be a sub-population of patients needing extra support and guidance through the immediate post-operative period.

Connective tissue changes such as scarring [29] and Axillary Web Syndrome (AWS) [32], or cording, are other known contributory factors to arm morbidity. Large numbers of women are still reporting tightness of the breast scar (29.2%) and axillary scar (36.5%) at 1 year follow up [29]. These effects are likely to be enhanced in more aggressive treatment protocols which have been reported as a risk factor for shoulder morbidity and for acute postoperative pain. In the early stages of recovery the above mentioned postural adjustment may be made to reduce tension on the site, thereby reducing pain. However, these adjustments together with the effects of radiotherapy may lead to the long-term effects reported here.

Very few patients in this study presented with a clinical diagnosis from scans and no pattern could be seen in the SPADI scores for patients with a diagnosed pathology. It would appear therefore that pain and loss of function is not coming from any overt structural pathology. This however, does need further clarification, as this report did not look at the connective tissue, vascular or neural changes in the axilla, clavicular and other regions. Vascular and fibrotic changes have been noted and could lead to the observations of weakness and fatigue [33, 34]. In light of the current findings, an in depth analysis of the scans and adjuvant treatment protocols is being undertaken.

Conclusion

Patients treated for breast cancer demonstrate altered muscle activity in three key muscles acting at the shoulder, reduced muscle size in two muscles in the line of surgery and radiotherapy, and persistent pain and functional limitation for up to 6 years after

treatment. These results suggest that the normal biomechanics of the shoulder complex is altered. Our laboratory is currently analysing the kinematic data for the glenohumeral joint and the scapula, which should provide further guidance in developing the exercise component of a rehabilitation programme.

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